

1 Study Protocol

2 Effect of restorative crown of different cuspal inclination and occlusal contact on stress
3 distribution in mandibular second premolar with different ferrule configuration and
4 peripheral bone- 3D finite element analysis

5 **Abstract**

6 **Background**

7 Restoration of pulpless teeth have been difficult because of coronal loss from dental
8 caries, diminished moisture content, endodontic therapy and fractures, resulting in
9 prone to fracture of the tooth during function .Cast metallic band enclosing around
10 cervical surface of a tooth is called ferrule. The role of ferrule is to assist in
11 strengthening the endodontically treated tooth.

12 **Purpose**

13 In case of ferrule less tooth, the post performs as a wedge and may result in root
14 fracture. Therefore modification in design of ferrule is required. Presence or absence of
15 ferrule of coronal dentin influenced stress distribution pattern within tooth structure.
16 Failure or success of a restoration may be influenced by on how the stress is dispersed
17 to the tooth structure so it is essential to study the stress dispersal pattern within tooth
18 and associated structure.

19 **Materials and methods**

20 A three-dimensional FE method (FEM) will be carried out for study and finite element
21 structural analysis programs will be HYPERMESH 11 and ANSYS 18.1 software.
22 Eight 3D models will be created to simulate endodontically restored mandibular second
23 premolar with different coronal dentin configurations. The complete crown will be
24 modeled with a 20-degree, 33- degree, 45-degree facial cusp inclination. The oblique
25 force of 200 N will be executed to the buccal cusp of mandibular second premolar.
26 Analysis of results will be done by both color-coding and numerically. By using FEA
27 software the von Mises equivalent stress (MPa) will be calculated

28

29 Key words - ferrule, post and core, finite element analysis, cuspal angulation

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31

32 **Introduction**

33 Nowadays restoration of pulpless tooth is quiet a controversial subject.
34 Due to dental structure damage, cavity preparation and root canal procedure those
35 teeth are weakened. (1)

36 Special care recommended while selecting the furthestmost competent way
37 to repair them. Cervical area of an endodontically treated tooth is most prone area for
38 maximum stress generation due to occlusal force. (2) **Post plays important role in**
39 **reduction of stress in cervical area of tooth as it distribute force along the post length.**
40 Therefore, post plays vital role in maintaining the remaining tooth structures

41 Successful result with restorative dentistry can be accomplished with
42 understanding of the importance of occlusion and not just depending on resilient
43 materials. The use of resilient materials may reduce the importance of an accurate
44 occlusion, which is hazardous to the overall periodontal structure. To preserve the
45 health of the masticatory system by managing occlusal discrepancy plays very
46 important role in restorative dentistry. (3-5) All root treated teeth should be restored
47 with prosthesis to protect the remaining cusps while mastication. Vertical root fracture
48 may occur due to lateral forces which can shear the residual cusp. (6) While
49 restoring pulpless tooth, a judgment regarding post placement is made based on the
50 functional necessities of the tooth, the residual coronal tooth structure and the loads
51 on the tooth. To make best use of the ferrule effect, dentist should preserve most of
52 coronal tooth structure as while preparing pulpless teeth. To obtain determined ferrule
53 effect the nominal height of 1.5-2 mm of whole tooth above the finish line, along
54 the circumference of the tooth preparation required. Mechanical resistance of the
55 tooth enhanced by dispensing forces on the residual tooth structure and thereby
56 increasing fracture resistance by maintaining the bond of the post/core or crown to the
57 tooth. (7) **Stress analysis is becoming interesting topic in dentistry for the past few**
58 **decades. To investigate very irregular and complex structures, finite element method**
59 **is popularly used method. Efficiency and versatility of this method already utilized in**

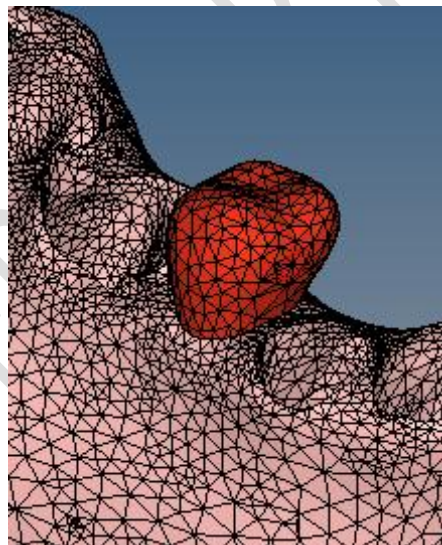
60 various fields like aeronautical, civil and mechanical engineering. (2) Moreover, finite
61 element method has extensive application in biomechanical branches like dentistry
62 and orthopedics.

63 By utilizing of 3- dimensional (3D) simulations with finite element method, the
64 study intended to evaluate effect of occlusal contact position, type of occlusal contact
65 and cuspal angulation on stress distribution in root treated second mandibular
66 premolar with dissimilar ferrule configurations.

67

68 **Materials and Methodology:**

69 It is in vitro computerized study, the experiments are repeatable and design of study
70 may be changed and modified as per the necessity. The study will be carried out using
71 the 3D simulations with finite element method (FEM) and for 3D meshing finite
72 element structural analysis programs will be HYPERMESH 11 and for load application
73 and problem solving ANSYS 18.1 software.



74

75 Image 1. FEA model of mandibular second premolar after meshwork

76 Various scientific studies observed the biomechanical behavior of anterior teeth after
77 restoration with intraradicular retainers and submitted to oriented loads. very little is
78 known about the biomechanical behavior of posterior teeth restored with intraradicular
79 retainers. In this Present Study, biomechanical characteristic of mandibular second
80 premolar with different ferrule configuration and cuspal angulation , occlusal contact
81 and different post material on stress distribution with FEA will be analysed.

82 A 3D model of posterior mandibular bone will be constructed. Endodontically treated
83 mandibular second premolar will be modelled with cancellous center bounded by
84 2-mm cortical bone of 16-mm width and 24-mm length (Image 1) The shape of
85 mandibular second premolar will be acquired by micro CT scan (SIRONA SCAN,
86 BELGIUM). The scanned profile will be assembled in 3D structure using 3D imaging
87 software (ANSYS 18.1) by measuring root form geometry of teeth. Ceramic material
88 used for final restoration of tooth. With 22.5 mm long tooth length and 12 mm length,
89 1.2 mm width of post will be modelled with Gutta-percha filling left 4 mm apically.

90 **Loading conditions**

91 To analyze the stress distribution, 200 N force in oblique direction is determined from
92 the literature, angled at 45 degrees, will be executed on a smaller area of the buccal cusp
93 to replicate the masticatory force

94 **Material properties**

95 2 mm thickness of porcelain fused with metal will be modelled in this study. All
96 materials were recognized as homogeneous, linear, isotropic and elastic. Elastic
97 properties such as Poisson ratio (μ) and Young's modulus (E) were decided from
98 literature. (8) Eight 3D models will be created to simulate endodontically restored
99 mandibular premolars with different ferrule configurations as follows:

- 100 1) Tooth with 4 mm remaining coronal (CC)
- 101 2) Tooth with complete circumferential 2 mm ferrule (CF)
- 102 3) Tooth with one walled buccal 2-mm ferrule (BF)
- 103 4) Tooth with one walled lingual 2-mm ferrule (LF)
- 104 5) Tooth with two walled buccal-lingual 2-mm ferrule(BLF)
- 105 6) Tooth with one walled proximal 2-mm ferrule (PF)
- 106 7) Tooth with three walled buccal -lingual-mesial 2-mm ferrule(BLMF)
- 107 8) Tooth with no ferrule. (NF)

108 For the reconstruction of the core composite resins material were chosen, that increases
109 fracture resistance and modulus of elasticity, also it reduces polymerization
110 contraction, coefficient of thermal expansion and water absorption. The models
111 treated with a post and core and a complete crown will be from 2 to 8, while the CC
112 tooth will be treated with a single complete crown. Fiber post material assumed to be
113 perfectly bonded to the root dentin.

114 **Cuspal angulation**

115 Cuspal angulation of final prosthesis will be with a 20-degree, 33- degree, 45-degree
116 facial cusp inclination.

117 **Location of contact**

118 An oblique load will be executed to the bottom, middle and top of the buccal cusp.

119 **Type of contact:**

120 1) Surface contact (2mm diameter)

121 2) Point contact (0.5 mm diameter)

122

123 **Expected outcome**

124 Ferrule effect in endodontically treated tooth has positive influence on stress
125 reduction. Occlusal anatomy and location of occlusal contact play important role in
126 favorable stress distribution.

127

128 **Interpretation of the FEA results**

129 Analysis and interpretation will be done by both numerically and color-coding. The
130 stress in form of the von Mises equivalent will be computed using FEA software
131 (ANSYS 18.1). All figures of maximum von Mises equivalent stress on the restored
132 tooth and associated structure will be charted and investigated for computation of the
133 results. Stresses in terms of von Mises yields an operative absolute magnitude of
134 stresses, considering principal stresses in three dimensions.

135 In the finite element model stress dispersion represented in color coding with numerical
136 values. Red color denotes maximum and blue represents minimum value of Von Mises
137 stress. Yellowish red, greenish yellow, green, bluish green in the descending order
138 represents in between values of stress distribution. (Image 2)

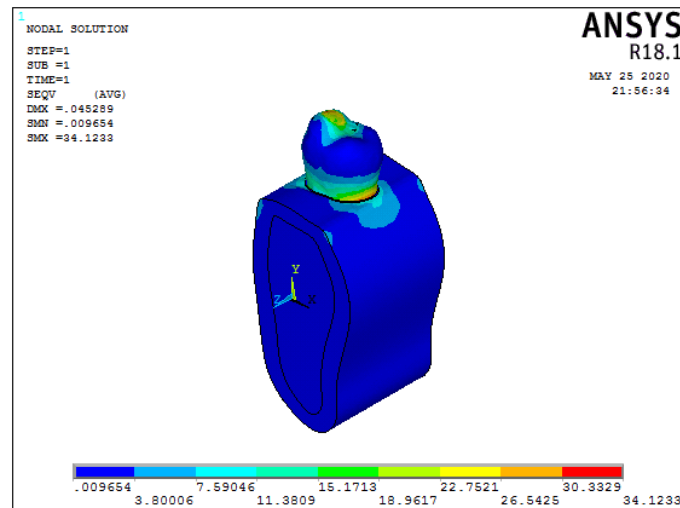


Image 2. FEA model representing color coding with numerical values of stress distribution

Von Mises measure is valid for the ductile materials which is having equivalent compressive or tensile strength. In case of materials like ceramics, cements or resin composites reported greater compressive strength than tensile strength, exhibiting brittle behavior. (14). Tensile or compressive stresses specified by positive and negative values at matching region. (15)

In case of asymmetrical loading the response of the structure will be different. Because of the higher compressive yield strength insignificant displacement seen in tooth when compressively loaded. In case of asymmetrical loading the tensile stress occurs. The tooth and associated structure are more resistant to compressive loads as compared to tensile forces which may induce a lesion in tooth structure. Lateral loads generate higher value of tensile stresses as compared to vertical loads. Due to tensile stresses, most of the failures occurred in dental materials used for tooth restoration. Very Specific occlusal modifications of teeth should be executed to avoid such events. (16)

157 LIMITATIONS

158 The precision of the simulated mathematical model of tooth and associated structures
159 decides the accuracy of analysis. All materials are measured as homogeneous and have
160 a linear reaction to stress contradictory to actual clinical condition. Clinically, the stress
161 reaction to these structures to is more complex. Here obliquely applied static loads will
162 be anticipated instead of realistic dynamic cyclic loads concentrating at tooth surface
163 during mastication of food.

164 Conclusion :

165 To the best of our knowledge, very few studies conducted till on this topic. This study
166 will signify strategies for reducing the lateral masticatory forces and to improve
167 biomechanical behavior. In group function circumstances, mandibular premolars which
168 are exposed to frequent oblique occlusal forces that are interpreted into high lateral
169 forces , occlusal design should be revised for teeth with significant dentin loss to protect
170 the supporting units and the restoration from overload. Modification in occlusal design
171 done by changing cuspal inclination. Importance of ferrule design will be investigated
172 to increase longitivity of endodontically treated tooth. Further study also will be
173 conducted by investigator and co-investigators.

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