

Original Research Article

Dosimetric Comparison of Stereotactic Body Radiotherapy in Lung Cancers: CyberKnife Versus Helical Tomotherapy Versus Volumetric Modulated Arc Therapy

ABSTRACT

Aim: Stereotactic body radiotherapy (SBRT) is widely used in the treatment of early-stage lung cancer. There are several SBRT techniques. We aimed to compare three planning techniques: CyberKnife (CK), Helical Tomotherapy (HT), and Volumetric Modulated Arc Therapy (VMAT).

Material and Methods: This study included 15 patients with early-stage lung cancer who were treated in our clinic. For this study, the images obtained were recontoured and replanned in CK, HT, and VMAT. Treatment plans were compared in terms of target volume and organ-at-risk doses.

Results: The HT plan differed significantly from the other plans in terms of conformity (CI), and gradient indexes (GI) ($p < 0.001$). There was a significant difference between the plans in terms of homogeneity indexes (HI) favoring HT ($p < 0.001$). VMAT plan reduced the monitor unit per fraction and beam on time per fraction values ($p < 0.001$). The lowest lung V5 (22.7%, $p = 0.046$), D_{max} , and the dose of 5 cc of trachea (499.4 cGy vs 252.4 cGy; $p = 0.017$, $p = 0.034$) and esophagus (673.9 cGy vs 237.3 cGy; $p = 0.014$ and $p = 0.08$) were observed with the VMAT plan.

Conclusions: All plans met the organ-at-risk dose constraints and target volume doses with acceptable limits. Each clinic should select an appropriate technique based on the available resources and experience.

Keywords: Lung cancer, Stereotactic body radiotherapy, CyberKnife, Helical tomotherapy, Volumetric modulated arc therapy

INTRODUCTION

Lung cancer is the leading cause of cancer-related death (18%) globally.[1] Currently, stereotactic body radiotherapy (SBRT) is the standard treatment method for medically inoperable early-stage lung cancers. High SBRT doses can be safely delivered with advanced techniques that provide high coherent target coverage and strict protection of adjacent normal tissues, and organs. Lee et al. reported that these techniques provided better local control with higher biologically effective dose values.[2], Prospective multi-institutional trials using SBRT have demonstrated local control and overall survival rates of approximately 85% and 60%, respectively.[3-5] SBRT is a treatment option without compromising the patient's quality of life, tolerable toxicity profile, and with a higher local disease control rate ($\geq 90\%$).[6] A study evaluated the cost-effectiveness of treatment modalities in patients with stage I non-small cell lung cancer (NSCLC) and revealed that SBRT was more cost-effective in marginally operable patients, whereas lobectomy was more cost-effective in clearly operable patients.[7]

CyberKnife (CK) is a robotic arm-mounted 6-MV linear accelerator image-guided radiotherapy system. Mobile tumors can be treated using this system with sub-millimeter accuracy in freely breathing patients. Helical tomotherapy (HT) is a technology that delivers image-guided intensity-modulated radiotherapy (IMRT), and treatment plans are generated in the Tomotherapy Hi-Art[®] planning system using 6-MV photons. Volumetric modulated arc therapy (VMAT) is an arc-based therapy that is delivered by a conventional linear accelerator.

This study aimed to compare the dosimetric differences between SBRT plans delivered with CK, HT, and VMAT in terms of quality and planning rationality for patients with early-stage NSCLC.

MATERIAL AND METHODS

47 In this study, the treatment of 15 patients with peripherally located early-stage NSCLC who had
48 previously undergone SBRT in our radiation oncology department was replanned using three
49 treatment planning systems (CK, HT, and VMAT) based on the same planning tomography. Patients
50 breathed freely and consistently during the procedure. Treatment planning using computed tomography
51 (CT) with a four-dimensional technique and 1.5-mm slice thickness was obtained for the delineation of
52 target volumes and organs-at-risk (OARs) using a multislice CT scanner (Philips Big Bore Brilliance CT
53 scanner (Philips Medical Systems, Cleveland, OH, USA)). After CT scanning, the CT data were
54 sorted into 10 breathing phases. The obtained CT dataset was sent to CK's planning system. All
55 patients were treated with CK. These CT data were transferred to the HT and VMAT
56 planning systems. Hi-ART® 5.1.4 version of HT was used. All target volumes and OARs were
57 recontoured for each patient by the same radiation oncologist. Gross tumor volume (GTV) indicated
58 the gross demonstrable extent and location of the tumor defined in radiological screenings..

59 All patients underwent positron emission tomography (PET) CT before treatment, and GTV was
60 contoured using PET CT fusions. Internal target volume (ITV) was defined for all patients using the
61 sorted breathing phases on planning CT. Subsequently, for all plans, planning target volume (PTV)
62 was generated with 5-mm margins from all directions to ITV. The lungs, esophagus, rib, heart, proximal
63 bronchial tree, trachea, great vessels, and spinal canal were all at risk. Radiotherapy plans in the
64 planning systems were performed by a physicist who was familiar with the systems used in this study.
65 Three plans were performed for each patient in CK, HT, and VMAT. The prescription dose was 50 Gy
66 in 5 fractions. The PTV was optimized to cover at least 95% of the target volume with 100% of the
67 prescription dose. Treatment plans were designed to meet Timmerman's normal tissue dose
68 constraints.[8]

69 CK plans were generated using sequential optimization in Multiplan version 3.5. Two fixed circular
70 collimators and two to three shell constraints were used for each plan. The 76% to 80% isodose line
71 interval was prescribed for treatment doses. During treatment, the tumor was tracked using the Xsight
72 Lung Tracking System (XLTS).

73 VMAT plans were generated using the Varian Eclipse version 11.4 treatment planning system, and
74 dose calculation was performed using the AAA algorithm. All plans were based on two coplanar partial
75 arcs with multileaf collimators. The optimization resolution was 2.5 mm in all cases.

76 All contours and CT images for HT were transferred to the tomotherapy planning station (Accuray,
77 Sunnyvale, CA, USA). Then plans were generated, using a fixed jaw mode with a modulation factor of
78 2.0, a field width of 2.50 cm, and a pitch factor of 0.15–0.18 cm.

79 Planning target volume, organ-at-risk doses, and treatment plan quality were used to compare
80 treatment plans. D₂, D₅₀, D₉₈, D_{min}, D_{max}, and D_{mean} were calculated from the dose- volume
81 histograms (DVHs) of all plans for the planning target volume (PTV). V₅, V₁₀, V₂₀, and mean lung
82 dose for the lung; the dose of 0.35 cc of spinal cord volume; D_{max} and the dose of 5 cc of esophagus
83 volume for the esophagus; D_{max} and the dose of 15 cc of heart volume for the heart; D_{max} of great
84 vessel volume; D_{max} and the dose of 5 cc for the trachea and proximal bronchial tree; D_{maxi} and the
85 dose of 5 cc for the rib were analyzed. The conformity index (CI), dose homogeneity index (DHI),
86 gradient index (GI), beam-on-time per fraction (BOT/fx), and monitor unit per fraction MU/fx were used
87 to evaluate treatment plan quality.

88 The CI was calculated as follows:

$$89 \quad CI = \frac{V_{Rx}}{TV_{Rx}},$$

90 where TV_{Rx} indicates tumor volume receiving the prescribed dose and V_{Rx} indicates prescription
91 isodose volume.

92 The new CI (nCI) was calculated as follows:

$$93 \quad nCI = \frac{TV}{TV_{Rx}} \times \frac{V_{Rx}}{TV_{Rx}},$$

94 where TV indicates tumor volume (cc), TV_{Rx} indicates tumor volume receiving the prescribed dose,

95 and V_{RX} indicates the prescription isodose volume. [9] The reference value of CI and nCI is accepted
 96 as 1.

97 The DHI was calculated to quantitatively evaluate dose heterogeneity in the target tumor using the
 98 following formula:

99
$$DHI = \frac{D_{maximum}}{D_{prescribe}}$$

100 where D_{maxi} indicates maximum dose to the target volume and $D_{prescribe}$ indicates prescription dose to
 101 the target volume.[9]

102 The GI was calculated as follows:

103
$$GI = \frac{V_{\%50Rx}}{V_{Rx}}$$

104 where $V_{\%50Rx}$ indicates 50% of prescription isodose volume and V_{RX} indicates prescription isodose
 105 volume.[10]

106 Statistical analysis

107 Statistical Package for Social Sciences v 16 (SPSS, SPSS Inc., Chicago, IL, USA) was used for
 108 statistical analyses. From the target perspective, percentage and mean \pm standard deviation
 109 (mean \pm sd) in the course from the study perspective. The Shapiro–Wilk test was used to test the
 110 fitness of the variables to normal distribution. The reconstruction of the two alignments was performed
 111 using analysis of foci under normal conditions and analysis of variance for normal alignments. *P*-values
 112 of < 0.05 were set as the level of statistical significance.

113

114 **RESULTS**

115 All 15 patients with lung cancers had peripherally located tumors including tumors on the right upper
 116 (n=6), right middle (n=3), and left upper (n=6) lobes. The mean PTV was 41.8 ± 32.5 cc (min = 8.9,
 117 max = 124.5). All OARs with comparable target coverage dose limitations met the Radiation Therapy
 118 Oncology Group [11] and/or Timmerman protocol limits.[8]

119 Significant differences were observed between the plans in terms of PTV_{mini} and PTV_{D98}
 120 ($P < 0.01$), which may be due to the differences between VMAT and other plans. Moreover, there were
 121 significant differences among all plans in terms of PTV_{mean} , PTV_{max} , and PTV_{D2} ($P < 0.01$). There was
 122 a significant difference between the plans in terms of PTV_{D50} ($P < 0.01$), which stemmed from the
 123 difference between CK plan and the other two plans (Table 1).

124 **Table 1: Comparisons among CK, HT, and VMAT plans in terms of PTV, and DVH parameters**

	CK	HT	VMAT	P-value
	Mean \pm SD	Mean \pm SD	Mean \pm SD	
PTV_{min} (cGy)	4792.1 ± 109.7^a	4692.9 ± 179.1^a	4407.5 ± 156.5^b	<0.001*
PTV_{mean} (cGy)	5483.1 ± 89.0^a	5128.2 ± 60.9^b	5225.7 ± 31.8^c	<0.001*
PTV_{max} (cGy)	6320.8 ± 130.7^a	5285.1 ± 92.8^b	5570.4 ± 101.7^c	<0.001**
PTV_{D98} (cGy)	4990.7 ± 76.7^a	4948.9 ± 37.7^a	4864.1 ± 65.4^b	<0.001*
PTV_{D50} (cGy)	5444.6 ± 92.7^a	5169.3 ± 112.4^b	5246.2 ± 23.6^b	<0.001**
PTV_{D2} (cGy)	6085.2 ± 124.3^a	5232.8 ± 88.2^b	5376.7 ± 53.6^c	<0.001**

125 One way analysis of variance, *Kruskal-Wallis analysis, ^{a,b,c} Statistically significant differences between the
 126 groups

127 Abbreviations: DVH: dose volume histogram, CK: CyberKnife, HT: Helical tomotherapy, VMAT: volumetric
 128 modulated arc therapy, PTV: planning target volume.

129

130 The HT plan differed significantly from the other plans in terms of CI, nCI, and GI ($P < 0.001$). There
 131 was a significant difference between the plans in terms of HI ($P < 0.001$). This difference resulted from
 132 the difference between the CK plan and other plans. There was a significant difference between all
 133 plans in terms of MU/fx and BOT/fx (min, $P < 0.001$) (Table 2).

134

135 **Table 2: Dosimetric results of CI, nCI, HI, GI, MU/fx, and bot/fx**

	CK	HT	VMAT	P-value*
	Mean ± SD	Mean ± SD	Mean ± SD	
CI	1.16 ± .04 ^a	1.25 ± .08 ^b	1.15 ± .15 ^a	<0.001
nCI	1.18 ± .05 ^a	1.33 ± .12 ^b	1.15 ± .05 ^a	<0.001
HI	1.27 ± .03 ^a	1.07 ± .06 ^b	1.11 ± .03 ^b	<0.001
GI	4.64 ± .53 ^a	6.35 ± 1.01 ^b	5.00 ± .72 ^a	<0.001
mu/fx (mu)	6625.1 ± 858.0 ^a	10071.9 ± 1692.6 ^b	3352.8 ± 618.0 ^c	<0.001
bot/fx(min)	35.8 ± 3.9 ^a	11.7 ± 1.9 ^b	6.4 ± .6 ^c	<0.001

136 One way analysis of variance, *Kruskal-Wallis analysis, ^{a,b,c} Statistically significant differences between the
 137 groups
 138

139 Abbreviations: CK: CyberKnife, HT: Helical tomotherapy, VMAT: volumetric modulated arc therapy, HI:
 140 homogeneity index, CI: conformity index, nCI: new conformity index, GI: gradient index, MU/fx: monitor unit per
 141 fraction, bot/fx: beam- ontime per fraction.

142 Significant differences were noted between CK and VMAT plans in terms of lung V5 ($P = 0.046$),
 143 trachea D_{max} ($p = 0.017$), trachea 5 ($P = 0.034$), and esophageal 5 ($P = 0.008$) There was a significant
 144 difference between the VMAT and other plans in terms of esophageal D_{max} ($P < 0.014$). (Table 3).

145 **Table 3: Dosimetric comparisons for OARs**

	CK	HT	VMAT	P-value*
	Mean ± SD	Mean ± SD	Mean ± SD	
Mean lungs-ptv (cGy)	410.6 ± 223.0	448.5 ± 168.7	307.5 ± 149.5	0.104**
Lung V 5 (%)	34.3 ± 16.3 ^a	32.1 ± 12.2 ^{a,b}	22.7 ± 9.8 ^b	0.046**
Lung V 10 (%)	20.4 ± 13.3	23.9 ± 9.8	16.6 ± 9.0	0.136
Lung V 20 (%)	20.9 ± 42.1	12.0 ± 6.3	8.3 ± 6.1	0.069
Spinal cord D 0.35 cc (cGy)	731.7 ± 507.1	598.0 ± 468.2	700.7 ± 358.4	0.828
Heart D _{max} (cGy)	847.1 ± 711.4	976.1 ± 1283.6	731.1 ± 1193.3	0.242
Trachea D _{max} (cGy)	992.0 ± 534.5 ^a	790.5 ± 456.7 ^{a,b}	499.4 ± 340.4 ^b	0.017**
Trachea D 5 cc (cGy)	600.3 ± 480.5 ^a	441.4 ± 336.8 ^{a,b}	252.9 ± 165.2 ^b	0.034**
PBT D _{max} (cGy)	727.7 ± 952.6	905.5 ± 633.8	800.3 ± 934.2	0.283
Rib D _{max} (cGy)	4441.3 ± 1477.3	4918.5 ± 726.6	4858.3 ± 873.0	0.800
Rib D 5 cc (cGy)	2106.5 ± 1533.0	2361.9 ± 1316.2	2354.9 ± 896.7	0.824**
Esophagus D _{max} (cGy)	1005.3 ± 422.8 ^a	998.6 ± 341.1 ^a	673.9 ± 209.1 ^b	0.014**

Esophagus D 5 cc (cGy)	585.7 ± 360.8 ^a	445.8 ± 255.5 ^{a,b}	257.3 ± 171.5 ^b	0.008**
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146 One way analysis of variance, Kruskal-Wallis analysis, ^{a,b,c} Statistically significant differences between the
147 groups

148 Abbreviations: OAR: organ at risk, PBT: proximal bronchial tree, CK: CyberKnife, HT: Helical tomotherapy,
149 VMAT: volumetric modulated arc therapy

150

151 DISCUSSION

152 SBRT is a treatment option for medically inoperable lung cancer. Thanks to technological
153 advancements, SBRT can be currently applied in modern radiotherapy clinics. This study has focused
154 on three different SBRT techniques to determine target volumes and critical organ doses.

155 Three different RT devices (CyberKnife®, Helical Tomotherapy®, and VMAT) were compared, and
156 evaluated in a study regarding the efficacy and toxicity of lung SBRT techniques.[12] The cited study
157 compared the CK results of 111 patients, with those of other plans (HT and VMAT), and
158 demonstrated dosimetric benefit of CK with reduced mean lung dose (2.6 vs. 4.1 Gy, $P < 0.001$), V5
159 (13.5% vs. 19.9%, $P = 0.002$), and V20 (2.3% vs. 5.4%, $P < 0.001$). The above-mentioned study did
160 not report a clear-cut criterion for preferring one technique over the other, and the obtained
161 dosimetric parameters had no effect on toxicity.[12] Our study evaluated all OARs and revealed
162 statistically significant differences between SBRT techniques concerning lung V5, D_{max} and dose of 5 cc
163 of the trachea and esophageal volume. VMAT plan had lower lung V5 ($P = 0.046$), D_{max} and trachea V5
164 ($P = 0.017$, $P = 0.034$) and esophagus V5 ($P = 0.014$, $P = 0.08$). However, we did not evaluate
165 the plans regarding their toxicity profiles in order to assess the effect of dosimetric advantage on
166 toxicity. However, a more comprehensive study evaluating the effect of dosimetric data can be done.

167 Desphande et al. conducted a comparative study and revealed that VMAT delivered higher maximum
168 doses to the GTV and PTV and lower lung V5 than other plans. CK plans had higher CI compared to
169 VMAT plans (median: 1.19 vs. 1.10, $P < 0.00001$), but VMAT plans had higher HI than CK plans
170 (median: 1.30 vs. 1.25, $P < 0.001$).[13] In contrast to these findings, we reported higher CIs and HIs in
171 HT and CK plans. The CK and VMAT plans are more heterogeneous; therefore, the maximum dose
172 and DHI tend to increase as the dose is trapped more effectively in the PTV.

173 There have been numerous dosimetric comparison studies based on CK and VMAT plans on lung
174 SBRT. Shao et al. evaluated SBRT plans and compared CK and Eclipse plans for lung SBRT in terms
175 of duration of treatment. They reported that MU/tx and BOT/tx values were statistically higher in VMAT
176 plans. The BOT/tx for VMAT plans was 8 min shorter than that for CK plans ($t = 7.23$, $P = 0.000$).[14]
177 Although in our study VMAT plans have been realized within a shorter treatment period compared
178 to CK plans, it is not preferred in clinical practice because of the absence of a tumor tracking system on
179 the linear accelerator. In our clinic CK is the first choice for SBRT, because CK has a real-time tumor
180 tracking system.

181 Yu et al. compared treatment planning systems for lung SBRT using the CK Multiplan and Varian
182 Eclipse treatment planning systems as well as VMAT and knowledge-based VMAT and revealed that
183 CK plans showed the highest MUs ($P < 0.001$). HI was higher for CK plans than for other plans
184 ($P = 0.003$ and $P = 0.006$). Conversely, OAR sparing was superior in VMAT than in CK plans.[15] Our
185 results were consistent with this study.

186

187 CONCLUSION

188 In this study all three SBRT systems used for lung tumors yielded optimal results. The OAR and target
189 volume doses were comparable in all plans. When we compared these three planning methods, only
190 lung V10 was significantly better than VMAT in OARs, but it remained within the range of dose
191 constraints according to the guidelines for all plans. Since in our patients the tumors were located
192 in the periphery of the lungs, the OAR values were within the limits stipulated by the guidelines and did
193 not differ significantly among all three plans. Thus, these techniques can be used safely. For the
194 selection of SBRT technique, each clinic should consider dosimetric results and the available
195 resources for lung SBRT. Since CK has a real-time tumor tracking system, in our clinic we prefer to

196 use CK as lung SBRT, and recommend that clinics with available sources should evaluate priority
197 use of CK for lung SBRT.

198 ETHICAL APPROVAL

199 The study was approved by the Ethical Committee of Dr Abdurrahman Yurtaslan Oncology Training
200 and Research Hospital, Ankara, Turkey (approval number 2022-05/109) on May 26, 2022.

201
202 Consent

203 As per international standard or university standard, patient(s) written consent has been collected and
204 preserved by the author(s).

205

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UNDER PEER REVIEW